Introduction to MRI and fMRI

The magnet

Introduction to MRI

Field strength

Introduction to MRI

Field strength

Introduction to MRI

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Spontaneous Discharge of a Firearm in an MR Imaging Environment

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Field strength

Water

The approximate shape and charge distribution of water.

Note that the average electron density around the oxygen atom is about 10x that around the hydrogen atoms.

Other nuclei such as 13C, 19F, 31P, 23Na have a net nuclear spin and can be imaged in MRI.

www.lsbu.ac.uk/water/

Proton

Proton

Introduction to MRI

Protons in uniform B_0 field

As spins do not rotate in phase, the sum of all the microscopic magnetizations of each spin is a null macroscopic magnetization.

Alignment with B_0 field

B_0

3 per million parallel vs. anti-parallel at 1T

Larmor precession

ω_0

B_0

Spins in a static magnetic field precess

Larmor precession

Introduction to MRI

Larmor precession

ω_0

B_0

Resonance:
exchange of energy
between two systems
at a specific frequency.
Magnetic resonance:
interaction between spins
and electromagnetic
radiofrequency (RF).

Larmor precession

B_0

ω_0

Resonance: exchange of energy between two systems at a specific frequency.

Magnetic resonance: interaction between spins and electromagnetic radiofrequency (RF).

1946:

Energy applied at a resonant frequency is absorbed by matter, and the re-emission can be measured in detector coils.

Bloch

Purcell

Signal: excitation & relaxation

Excitation

90° RF pulse

Excitation

90° RF pulse

Introduction to MRI

Relaxation

Introduction to MRI

Relaxation

Relaxation

Introduction to MRI

Relaxation

T2* Free Induction Decay (FID)

Static inhomogeneities in magnetic fields accelerate spins dephasing.

Relaxation

RF pulses

90°   180°   180°   180°   180°

T2 decay

T2* decay

Relaxation

Signal

- 100 %
- 75 %
- 50 %
- **37 %**
- 25 %

Excitation

Relaxation

0 ms   **T2**   300 ms   450 ms   600 ms   **Time**

Decay of transverse magnetization, due to spins getting out of phase (spin-spin interactions), according to an exponential curve characterized by time constant T2.
T2 values are lower than T1 values and are unrelated to field strength.

Relaxation

Recovery of longitudinal magnetization, aligned with B_0,
following an exponential curve characterized by time constant T1.
With a 1.5 T field strength, T1 values are about 200 to 3000 ms.
T1 values are longer at higher field strengths.

T1-, T2-, PD-weighting

	P_D	T_2 (ms)	T_1 (ms)
White matter	0.61	67	510
Gray matter	0.69	77	760
CSF	1.00	280	2650

White matter

CSF

(a)

PD weighted

(b)

T2- weighted

(c)

T1- weighted

Gray matter

Tissue contrast

t = TR × [# phase encoding steps] × [# acquisitions to average]

Tissue contrast

Signal

difference due to
T1 relaxation

ms

Short TR

By setting the TR to short values, tissue contrast will depend
on differences in longitudinal magnetization recovery (T1).

Tissue contrast
(Spin-echo)

Signal

Short TR
Short TE

Long TR
Short TE

Long TR
Long TE

Short TR
Long TE

T2-weighted

Long TR   Long TE

ms

Tissue contrast
(Spin-echo)

Signal

Short TR
Short TE

Long TR
Short TE

Long
TR

Short TR
Long TE

Proton density

Long TR   Short TE

ms

Spatial encoding

Introduction to MRI

Spatial encoding

Head   Breast

Pelvic Phased-Array

Spatial encoding

Slice selection in z

Spatial encoding

K Space

Spin echo sequence

1. RF pulse + Slice select gradient

2. Phase encoding gradient

3. Frequency encoding gradient (dephasing lobe)

4. 180 RF pulse + Slice select gradient

5. Frequency encoding gradient + Signal recording

Parameters for Neuroimaging

You decide:
 number of slices
 slice orientation
 slice thickness
 in-plane resolution (field of view and matrix size)
 volume acquisition time (usually = TR)
 length of a run
 number of runs
 duration and sequence of epochs within each run
 counterbalancing within or between subjects

Your physicist can help you decide:
 pulse sequence (e.g., gradient echo vs. spin echo)
 k-space sampling (e.g., echo-planar vs. spiral imaging)
 TR, TE, flip angle, etc.

Frequency encoding

Introduction to MRI

Fourier analysis

Any wave form can be decomposed into a series of sine waves

Introduction to MRI

Fourier analysis

Introduction to MRI

Fourier analysis

spatial domain

magnitude

Introduction to MRI

Fourier analysis

frequency domain

spatial domain

magnitude

frequency

Introduction to MRI

Fourier analysis

frequency domain

spatial domain

magnitude

frequency

x

k-space

Introduction to MRI

k-space

K Space

Image

Introduction to MRI

k-space

K Space

Image

Introduction to MRI

k-space

K Space   Image

k-space

K Space   Image

k-space

K Space   Image

k-space

K Space   **Image**

k-space

K Space   **Image**

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K Space   **Image**

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Introduction to MRI

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k-space

Linear trajectory

Introduction to MRI

k-space

k-space

k-space

Introduction to MRI

MRI vs. fMRI

MRI

high resolution
(1 mm)

One 3D volume

fMRI

low resolution
(~3 mm)

∴

series of 3D volumes (i.e., 4D data)
(e.g., every 2 sec for 5 mins)

Category-Specific Visual Areas

objects

faces

places

Ventral view

RH   LH

Lateral view

LH

LOC   LO
pFs

Malach, 2002, TICS

- **Parahippocampal Place Area (PPA)**
  – place-selective
  – places > (objects and faces)
  – places > scrambled images

- **Lateral Occipital (LO)**
  – object-selective
  – objects > (faces & scenes)
  – objects > scrambled images

- **Fusiform Face Area (FFA) or pFs**
  – face-selective
  – faces > (objects & scenes)
  – faces > scrambled images
  – ~ posterior fusiform sulcus (pFs)

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fMRI Experiment Stages: Prep

1) **Prepare subject**

- Consent form
- Safety screening
- Instructions and practice trials if appropriate

2) **Shimming**

- putting body in magnetic field makes it non-uniform
- adjust 3 orthogonal weak magnets to make magnetic field as homogenous as possible

3) **Sagittals**

Take images along the midline to use to plan slices

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fMRI Experiment Stages: Anatomicals

4) Take anatomical (T1) images

- high-resolution images (e.g., 0.75 x 0.75 x 3.0 mm)
- 3D data: 3 spatial dimensions, sampled at one point in time
- 64 anatomical slices takes ~4 minutes

64 slices x
3 mm

Slice Terminology

SAG

A

P

SAGITTAL SLICE

Slice Thickness
e.g., 6 mm

Number of Slices
e.g., 10

VOXEL
(Volumetric Pixel)

In-plane resolution
e.g., 192 mm / 64
= 3 mm

3 mm

6 mm

3 mm

IN-PLANE SLICE

Matrix Size
e.g., 64 x 64

Field of View (FOV)
e.g., 19.2 cm

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fMRI Experiment Stages: Functionals

5) Take functional (T2*) images

- images are indirectly related to neural activity
- usually low resolution images (3 x 3 x 6 mm)
- all slices at one time = a volume (sometimes also called an image)
- sample many volumes (time points) (e.g., 1 volume every 2 seconds for 136 volumes = 272 sec = 4:32)
- 4D data: 3 spatial, 1 temporal

fMRI Simplified

ROI Time Course

fMRI Signal Intensity

Time

Condition

~2s

16.00

10.03

t(126)

p < 9.3347e-18

Condition 1

Time

Condition 2

Region of interest (ROI)

~ 5 min

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A Simple Experiment: LO Localizer

Lateral Occipital Complex
• responds when subject views objects

Blank Screen

Intact Objects

TIME ➡

Scrambled Objects

One volume (12 slices) every 2 seconds for 272 seconds (4 minutes, 32 seconds)

Condition changes every 16 seconds (8 volumes)

Design Jargon: Runs

session: all of the scans collected from one subject in one day

run (or scan): one continuous period of fMRI scanning (~5-7 min)

experiment: a set of conditions you want to compare to each other

condition: one set of stimuli or one task

2 stimulus conditions
+ 1 baseline condition (fixation)

A session consists of one or more experiments.
Each experiment consists of several (e.g., 1-8) runs

Design Jargon: Paradigm

paradigm (or protocol): the set of conditions and their order used in a particular run

epoch: one instance of a condition

- first "intact objects" epoch
- first "scrambled objects" epoch
- second "intact objects" epoch

run

volume #1 (time = 0)

epoch 8 vol x 2 sec/vol = 16 sec

volume #136 (time = 136 vol x 2 sec/vol = 272 sec = 4:32)

Time

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Statistical Maps & Time Courses

Use stat maps to pick regions

Then extract the time course

Stats on Anatomical

2D ➔ 3D

Sample Artifacts

Ghosts

Hardware Malfunctions

Metallic Objects (e.g., hair tie)

Spikes

What affects SNR?
Physiological factors

PHYSIOLOGICAL FACTORS	SOLUTION & TRADEOFF

Head (and body) motion	Use experienced or well-warned subjects
	    – limits useable subjects
	Use head-restraint system
	    – possible subject discomfort
	Post-processing correction
	    – often incompletely effective
	    – 2nd order effects
	    – can introduce other artifacts
	Single trials to avoid body motion

Cardiac and respiratory noise	Monitor and compensate – hassle
Low frequency noise	Use smart design Perform post-processing filtering
BOLD noise (neural and vascular fluctuations)	Use many trials to average out variability
Behavioral variations	Use well-controlled paradigm Use many trials to average out variability

Source: Doug Noll's online tutorial

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Find the "Sweet Spots"

Respiration
• every 4-10 sec (0.3 Hz)
• moving chest distorts susceptibility

Cardiac Cycle
• every ~1 sec (0.9 Hz)
• pulsing motion, blood changes

Solutions
• gating
• avoiding paradigms at those frequencies

You want your paradigm frequency to be in a "sweet spot" away from the noise

Data Preprocessing Options

reconstruction from raw k-space data
- frequency space → real space

artifact screening
- ensure the data is free from scanner and subject artifacts

vessel suppression
- reduce the effects of large vessels (which are further away from activation than capillaries)

slice scan time correction
- correct for sampling of different slices at different times

motion correction
- correct for sampling of different slices at different times

spatial filtering
- smooth the spatial data

temporal filtering
- remove low frequency drifts (e.g., linear trends)
- remove high frequency noise (not recommended because it increases temporal autocorrelation and artificially inflates statistics)

spatial normalization
- put data in standard space (Talairach or MNI Space)

Links

http://www.cis.rit.edu/htbooks/mri/inside.htm

http://www.e-mri.org/

http://www.cis.rit.edu/htbooks/mri/inside.htm

http://www.simplyphysics.com

http://www.hull.ac.uk/mri/lectures/gpl_page.html

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http://eeweb.poly.edu/~yao/EL5823/MRI_physics_ch12.pdf

http://web2.uwindsor.ca/courses/physics/high_schools/2006/Medical_Imaging/
mriphysics1.html