RAPID COMMUNICATION

Novel Porcine Model of Acute Severe Cardiogenic Shock Developed by Upper-Body Hypoxia

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Summary

Despite the urgent need for experimental research in the field of acute heart failure and, particularly cardiogenic shock, currently there are only limited options in large animal models enabling research using devices applied to human subjects. The majority of available models are either associated with an unacceptably high rate of acute mortality or are incapable of developing sufficient severity of acute heart failure. The objective of our research was to develop a novel large animal model of acute severe cardiogenic shock. Advanced left ventricular dysfunction was induced by global myocardial hypoxia by perfusing the upper body (including coronary arteries) with deoxygenated venous blood. The model was tested in 12 pigs: cardiogenic shock with signs of tissue hypoxia developed in all animals with no acute mortality. Cardiac output decreased from a mean ($\pm$ SD) of 6.61 ± 1.14 l/min to 2.75 ± 0.63 l/min, stroke volume from 79.7 ± 9.8 ml to 25.3 ± 7.8 ml and left ventricular ejection fraction from 61.2 ± 4.3 % to 17.7 ± 4.8 % ($P \leq 0.001$ for all comparisons). In conclusion, the porcine model of acute cardiogenic shock developed in the present study may provide a basis for studying severe left ventricular dysfunction, low cardiac output and hypotension in large animals. The global myocardial hypoxia responsible for the decrease in cardiac contractility was not associated with acute death in this model.

Key words

Acute heart failure • Animal model • Cardiogenic shock • Extracorporeal life support • Extracorporeal membrane oxygenation • Pig

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Recent advances in the development of minimally invasive mechanical cardiac or circulatory support systems for the treatment of acute severe or rapidly progressing cardiogenic shock have prompted the urgent need for relevant animal models in preclinical testing. However, currently available options in large animals (e.g. dogs, pigs, sheep), in which instrumentation used on humans can be applied, are significantly limited. To date, several methods to induce acute left ventricular (LV) dysfunction (e.g. coronary microsphere embolization, coronary ligation or coronary obstruction by angioplasty balloon inflation) have been described in these large animal species (Abarbanell *et al.* 2010, Dixon and Spinale 2009, Schmitto *et al.* 2011). Development of sufficient myocardial ischemia leading to cardiogenic shock (i.e. left anterior descending artery occlusion) is, however, associated with high acute mortality, reaching up to 70 % due to the induction of refractory ventricular fibrillation (Franciosa *et al.* 1980, Smiseth *et al.* 1983). Reduction of ischemic time or smaller coronary artery obstruction does not produce sufficiently severe heart failure leading to the development of cardiogenic shock, and is frequently followed by rapid restoration of LV function (Lindal *et al.* 1986, Moainie *et al.* 2002, Schmitto *et al.* 2009, 2011, 2008). Currently, a large

animal model of acute severe cardiogenic shock with reasonably low mortality is lacking. Accordingly, we recently induced acute cardiogenic shock by selective perfusion of the left anterior descending artery with deoxygenated venous blood in a porcine model (Ostadal *et al.* 2015); however, the extent of LV dysfunction achieved was highly dependent on the coronary anatomy. The aim of the present study was, therefore, to develop a fully predictable and reproducible large animal model of acute cardiogenic shock induced by coronary perfusion with deoxygenated blood with acceptably low mortality.

Animal model. Twelve female swine (*Sus scrofa domestica*, Large White x Landrace crossbreed), four to five months of age, with a mean body weight of 45 kg were used to develop the model. After a 24 h fasting, general anesthesia was induced by administration of midazolam (0.3 mg/kg intramuscular) and ketamine hydrochloride (15 mg/kg to 20 mg/kg intramuscular). Initial propofol and morphine boluses (2 mg/kg intravenous [IV] and 0.1 mg/kg to 0.2 mg/kg IV, respectively) were administered, and the animals were orotracheally intubated. Continuous IV infusions of propofol (8 mg/kg/h to 10 mg/kg/h) and morphine (0.1 mg/kg/h to 0.2 mg/kg/h) were used to maintain anesthesia. The doses were adjusted according to physiological parameters, photoreaction, corneal and palpebral reflexes, lacrimation and spontaneous movement. Potassium chloride (2 mEq/kg), in conjunction with general anesthesia, was used to euthanize the animals at the conclusion of the experiment.

Bilateral femoral (arterial and venous), carotid and jugular approaches were used for multiple sheath insertions using the standard percutaneous Seldinger technique. An initial rapid IV infusion of 1000 ml normal saline was administered after anesthesia induction, followed by a continuous IV drip at a rate of 100 ml/h to 500 ml/h to reach and maintain a mean right atrial pressure of 5 mm Hg to 7 mm Hg. An unfractionated heparin bolus (100 U/kg IV) was administered after sheath placement, followed by a continuous IV infusion of 50 U/kg/h to maintain an activated clotting time of 180 s to 250 s. Values were monitored every hour using the Hemochron Junior Signature Plus Microcoagulation System (ITC, USA).

Ventilation was provided using a ventilator (Hamilton G5, Hamilton Medical AG, Switzerland) set to the INTELLiVENT – Adaptive Support Ventilation mode. The ventilator was set to maintain an oxygen

saturation (SpO₂) of 95 % to 99 %, and an end-tidal CO₂ pressure of 4.8 kPa to 5.6 kPa.

Veno-arterial extracorporeal membrane oxygenation (ECMO) circuit consisted of a Levitronix Centrimag (Thoratec, USA) or Maquet Rotaflow (Maquet, Germany) console and centrifugal pump, a tubing set (HMO 70000 Adult Microporous Membrane Oxygenator with Softline Coating [MAQUET Cardiopulmonary AG, Germany]) and a mechanical gas blender (Sechrist, USA). Cannulas (Maquet, Germany) were inserted percutaneously using the standard Seldinger technique into the femoral artery and vein. The venous inflow cannula (21 Fr or 23 Fr) was inserted into the right atrium (the tip position was verified using fluoroscopy), and the femoral arterial outflow cannula (15 Fr or 17 Fr) was inserted into the femoral artery. Blood gas parameters in the blood leaving the oxygenator were continuously monitored (CDI™ Blood Parameter Monitoring System 500, Terumo Cardiovascular Systems Corporation, USA). The oxygen/air flow was repeatedly adjusted to maintain a partial pressure of oxygen (PaO₂) and partial pressure of carbon dioxide (PaCO₂) in the ranges of 10 kPa to 15 kPa, and 4.0 kPa to 6.5 kPa, respectively. The extracorporeal blood flow (EBF) was set to 1 l/min until the start of the experiment.

Vital function and hemodynamic monitoring. Arterial pressure was measured using standard invasive methods with fluid-filled pressure transducers (Truwave, Edwards Lifesciences, LLC, USA) through a pigtail catheter inserted into the aortic arch. A Swan-Ganz catheter was inserted *via* a femoral vein to the pulmonary artery. Electrocardiography, heart rate (HR), invasive blood pressures (aortic arch and central vein), pulse oximetry, capnometry and invasive central venous SpO₂ were continuously monitored in all animals (Monitor Life Scope TR, Nihon Kohden, Japan; and Vigilance II, Edwards Lifesciences, USA). Brain and peripheral tissue oxygenation levels were measured using near-infrared spectroscopy (INVOS Cerebral/Somatic Oximeter, Somanetics, USA).

Pressure-volume (PV) analysis. PV conductance catheter (Scisense 7F VSL Pigtail, Transonic, USA) was inserted into the left ventricle from the left carotid artery through the aortic valve to monitor cardiac performance during cardiogenic shock induction and maintenance. Correct positioning was assessed radiographically by confirming

Fig. 1. Schematic illustration of the experimental settings. RA, right atrium; FA, femoral artery; FV, femoral vein

optimal PV loop morphology. The catheter was connected to the PV unit (Sciense ADV 500, Transonic, USA) and operated in admittance mode. The volume was calibrated against pulmonary thermodilution (Combo CCO catheter, Edwards Lifesciences, USA) at baseline. PV values were recorded continuously during the experiment. Collected PV data included end-diastolic pressure (EDP), end-diastolic volume (EDV), systolic blood pressure (SBP) and end-systolic volume (ESV). Stroke volume (SV) was calculated as $SV = EDV - ESV$; left ventricular ejection fraction (LVEF) was calculated as $LVEF = SV/EDV$; and cardiac output (CO) was calculated as $CO = SV \times HR$.

Cardiogenic shock development. After initiation of ECMO, the animals were stabilized for 10 min. Artificial ventilation was subsequently switched to the CMV mode at 5 breaths/min, 100 ml inspiration volume and a fraction of inspired oxygen (FiO_2) of 0.21, which caused severe hypoxemia in the blood entering the left heart chambers and causing tissue hypoxia in all tissues perfused by LV cardiac output, i.e. upper (front) body including the coronary arteries, similarly to the clinical conditions known as “Harlequin syndrome” (Fig. 1). Subsequent global myocardial hypoxia rapidly lowered

cardiac contractility, LVEF and blood pressure. At the same time, however, the lower body was perfused with fully oxygenated blood from ECMO entering the circulation via the femoral artery. During the hypoxic period, EBF was gradually increased to maintain a mean arterial pressure >60 mm Hg, ensuring adequate perfusion pressure. With the increasing EBF and decreasing LV cardiac output resulting from impaired myocardial contractility (increased EBF/LV cardiac output ratio) also substantially larger part of the body was perfused with oxygenated blood coming from ECMO. After approximately 1 h of myocardial hypoxia, the hemodynamic criteria for severe cardiogenic shock were met, including LVEF that decreased to $<30\%$ and CO to <3.5 l/min. Thereafter, continuous heart perfusion with hypoxemic blood enabled the maintenance of advanced myocardial dysfunction and severely compromised hemodynamic parameters. If cardiac performance parameters decreased further with a risk of circulation collapse, the target level of cardiogenic shock severity was adjusted by a partial increase in ventilation.

Severe cardiogenic shock was successfully induced in all 12 animals, with no need for cardioversion/defibrillation and zero acute mortality. The achieved hemodynamic and cardiac performance values

Table 1. Major hemodynamic and left ventricular performance parameters at baseline and after development of cardiogenic shock.

Parameter	Baseline	Cardiogenic shock	P
End-diastolic volume, ml	130.0±11.0	142.0±13.3	0.073
End-systolic volume, ml	50.3±6.3	116.6±11.9	<0.001
Stroke volume, ml	79.7±9.8	25.3±7.8	<0.001
End-diastolic pressure, mm Hg	13.6±2.3	28.1±5.8	<0.001
Systolic pressure, mm Hg	115.7±8.2	63.5±22.2	<0.001
Left ventricular ejection fraction, %	61.2±4.3	17.7±4.8	<0.001
Heart rate, beats/min	82.8±9.8	112.0±16.1	<0.001
Cardiac output, l/min	6.61±1.14	2.75±0.63	0.001

Data presented as mean ± SD unless otherwise indicated

at minimal ECMO flow (1 l/min) are shown in Table 1: CO decreased from 6.61±1.14 l/min to 2.75±0.63 l/min, SV from 79.7±9.8 ml to 25.3±7.8 ml, and LVEF from 61.2±4.3 % to 17.7±4.8 %.

Our novel large animal model of acute severe cardiogenic shock has several limitations. First, ECMO initiation is required for the maintenance of adequate perfusion pressure and for perfusion of fully oxygenated blood to a substantial part of the body. This approach, however, afforded sufficient time for the induction of significant LV dysfunction. Moreover, LV ejections not only supply coronary arteries with hypoxemic blood, but, at least during the initial phases of a hypoxic period, other tissues, including the brain, as well, similarly to the circulatory conditions in “Harlequin syndrome”; therefore, cerebral damage could be anticipated. We cannot exclude the possibility that central nervous system hypoxia may have impaired some of the reflexes regulating blood circulation. Transient hypoxia of the upper body and continuing hypoxia in some tissues, i.e. right upper (front) limb, may also influence the circulatory conditions. This is one of the most important reasons why this model cannot be used generally for studying of all aspects and all etiologies of cardiogenic

shock. Furthermore, although all animals subjected to global myocardial hypoxia in our study survived and none experienced ventricular fibrillation or sustained ventricular tachycardia, we cannot exclude the possibility that this observation was due to a limited sample size.

In conclusions, we developed a novel porcine model of acute cardiogenic shock with severe and sustained LV dysfunction, low CO and hypotension. Global myocardial hypoxia responsible for a decrease in cardiac contractility did not cause malignant arrhythmia(s) and all animals survived. With all limitations stated above this model can be used for the studying of selected aspects of cardiogenic shock and for the hemodynamic efficacy testing of some mechanical circulatory support systems.

Conflict of Interest

There is no conflict of interest.

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