Effect of the viscosity ratio on the PLA/PA10.10 bioblends morphology and mechanical properties

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Abstract. PLA bio-blends with a predominantly biosourced PA10.10 in the composition range 10–50 wt% were prepared by melt blending in order to overcome the advanced brittleness of PLA. Due to the inherent immiscibility of the blends, 30 wt% of PA was needed to achieve a brittle-to-ductile transition and a co-continuous morphology was predicted at 58 wt% of PA. The initial enhancement of the PLA rheological behaviour through the environmentally friendly reactive extrusion process yielded a finer and more homogeneous microstructure and hence enhanced the mechanical properties of the bio-blends at much lower PA contents. The brittle-to-ductile transition could be achieved with only 10 wt% and co-continuity was observed already at 44 wt% of PA. Results indicate the significant potential of modifying PLA flow behaviour as a promising green manufacturing method toward expanding PLA-based bio-blends applications.

Keywords: biopolymers, rheology, material testing, mechanical properties

1. Introduction

Poly (lactic acid) (PLA) is the front runner in the emerging bio-based and compostable plastic market. Initially, PLA has been viewed as a good alternative to commercial polymers for commodity applications (i.e. packaging). Unfortunately, its advanced brittleness at room temperature (*RT*) has been its major disadvantage for its implementation into high-value and durable applications (i.e. electronic or automotive). Blending PLA with other engineering soft polymers represents an industrially relevant strategy for developing bio-based formulations with tailored performances [1]. Specifically, numerous works report the investigation of melt blending PLA with polyamides (PA) [2–7]. However, the inherent immiscibility of this binary polymer system results in rather poor

mechanical properties. To overcome the aforementioned issue, Pai *et al.* [3] as well as Patel *et al.* [7] reported the first intents to compatibilize PLA/PA blends by adding titanium isopropoxide and a low molecular weight (M_w) epoxy resin, respectively. Unfortunately, a high PA content (≥ 50 wt%) is needed to change the blend morphology from droplet-matrix to co-continuous in order to improve the mechanical properties [4, 6, 7]. Therefore, PLA/PA blends with a predominant PLA content still exhibit brittleness. Polymer blends exhibiting a fine-tuned morphology with a significant reduced droplet size of the minor phase are promising due to their enhanced toughness in comparison to coarse sea-island morphologies [8]. Nuzzo *et al.* [6] reported the use of a third component (i.e. nanoparticles) in PLA/PA11 blends to both

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decrease the droplet size of the PA dispersed phase and to shift the onset of co-continuity towards lower PA amounts (30 wt%). However, mechanical properties are still far from being enhanced. In the case of selective positioning at the polymer-polymer interface, nanofillers act as stress concentrators; thus weakening the interfacial adhesion [6]. Moreover, the addition of nanoparticles is relatively complicated for large-scale productions. Hence, an on-line processing technique that offers control over both the minor phase size and morphology is a desirable alternative to tailor the mechanical properties of PLA/PA blends.

Among all available strategies enabling a process-controlled morphogenesis, the viscosity ratio of the blend, λ , i.e. the viscosity of the minor phase (η_{minor}) divided by that of the matrix phase (η_{major}) (in this case $\lambda = \eta_{\text{PA}}/\eta_{\text{PLA}}$), plays a major role in the final blend morphology [9–11]. Despite the general agreement in recognizing that usually $\eta_{\text{PA}}/\eta_{\text{PLA}} > 1$ [4], investigations relating the role of modifying the PLA rheological behaviour on the final PLA/PA blend morphologies remain unavailable, to the best of the authors' knowledge. The present work addresses these issues through a comparative study of bio-blends of a rheologically modified PLA (referred to as PLA_{REX}) and a green bio-based PA10.10. This commercially available PA grade was chosen because of its relatively low melting temperature; thus minimizing the well-known thermal degradations of PLA during processing [12]. Moreover, its green bio-based character highlights a research effort on the development of entirely bio-sourced blends to make the material suitable for a wider range of products. Specifically, reactive extrusion using a multifunctional epoxide reactive agent (referred to as SAMfE) was used to enhance the PLA flow behaviour in a pilot plant. Then, the effect of this tailored viscosity ratio on both the morphology and mechanical behaviour of these PLA_{REX}/PA bio-blends were investigated and compared to unmodified PLA/PA bio-blends.

2. Experimental

2.1. Materials

A commercially available extrusion-grade PLA (Ingeo 4032D®; D lactide content: 2%) was purchased from Natureworks (Arendonk, Belgium) and used as received. SAMfE reactive agent, namely Joncryl-ADR-4300F®, was kindly supplied by BASF (Ludwigshafen, Germany) with an epoxy equivalent

weight of 433 g·mol⁻¹ and a functionality of about 12. The predominantly bio-based PA10.10 was produced by Dupont (Midland, USA) under the trade name Zytel RS LC1000 BK385.

2.2. Reactive extrusion and sample preparation

The bio-blends were prepared using a two-step process. Prior to processing, raw PLA was dried at 80 °C for 4 h in a Piovani (DSN506HE, Venice, Italy) hopper-dryer (dew point = -40 °C). SAMfE flakes were vacuum-dried overnight at RT over silica gel. Initially, the enhancement of the PLA melt properties was achieved through reactive extrusion using a co-rotating twin-screw extruder with a screw diameter of 25 mm ($L/D = 36$) (KNETER 25X24D, Collin GmbH, Ebersberg, Germany) and a nominal SAMfE content of 0.6 wt%. The seven heating zones were set to 45, 165, 165, 170, 180, 190, 190 °C from the feeding zone to the die, respectively. The screw speed was set to 35 rpm; leading to a residence time of 4.1 min. A N₂ blanket was introduced in the hopper of the feeding zone and vacuum was applied to the metering zone. The extrudate (referred to as PLA_{REX}) was water-cooled and pelletized.

Then, five PLA_{REX}/PA blends, covering the 10–50 wt% PA composition range, were prepared by melt mixing using a Brabender batch mixer (Brabender Plastic-Corder W50EHT, Brabender GmbH&Co., Duisburg, Germany) operated at 210 °C and 50 rpm for 12 min under a N₂ blanket. The obtained materials

Table 1. Formulation and nomenclature of all investigated samples.

Sample nomenclature	PLA/PA [wt/wt]	PLA _{REX} /PA [wt/wt]
PLA	100/0	–
PLA _{REX}	–	100/0
PA	0/100	–
PLA-based bio-blends		
PLA90	90/10	–
PLA80	80/20	–
PLA70	70/30	–
PLA60	60/40	–
PLA50	50/50	–
PLA_{REX}-based bio-blends		
PLA _{REX} 90	–	90/10
PLA _{REX} 80	–	80/20
PLA _{REX} 70	–	70/30
PLA _{REX} 60	–	60/40
PLA _{REX} 50	–	50/50

were further compression moulded into 0.6 mm thick plates in an IQAP LAP PL-15 hot plate press (IQAP Masterbatch SL, Barcelona, Spain) for 5 min at 210 °C and 4 MPa and then cooled to RT at about –50 °C/min. Prior to processing, PLA_{REx} and PA were vacuum-dried overnight at 80 °C over silica gel. For the sake of comparison, five PLA/PA blends as well as the three pure polymers (i.e. PLA, PLA_{REx}, PA) were also manufactured using the same processing conditions. All prepared samples are summarized in Table 1.

2.3. Dynamic rheological measurements

The raw materials (i.e. PLA, PLA_{REx}, PA pellets) were rheologically characterized using an AR-G2 rheometer (TA Instruments, New Castle, DE, USA) under dry N₂ atmosphere in parallel plate (diameter = 25 mm) configuration with a constant gap of 1 mm. Prior to testing, pellets were vacuum-dried overnight at 55 °C over silica gel. Measurements were performed at small strains to ensure that the material's response was in the linear viscoelastic regime (LVR). Dynamic frequency sweeps were carried out at 210 °C (i.e. blend processing temperature), in the frequency (ω) range $0.0628 < \omega < 628 \text{ rad}\cdot\text{s}^{-1}$ under controlled deformation conditions (2%, LVR).

2.4. Size-exclusion chromatography (SEC)

The molecular weight distribution of the raw materials was determined at RT using an Agilent model Infinity 1260 SEC system (Agilent Technologies, Santa Clara, CA, USA) equipped with an Agilent PL HFIPgel (300×7.5 mm) specialist column (flow rate: 1 mL·min⁻¹) and a differential refractive index detection (SEC-DRI). Hexafluoroisopropanol (HFIP) containing 0.02 mol·L⁻¹ of sodium trifluoroacetate to prevent polyelectrolyte effect was used as eluent. Molar mass values (M_n and M_w being the number and weight average MW, respectively) were calculated by reference to a relative calibration curve obtained with poly(methyl methacrylate) standards.

2.5. Scanning electron microscopy (SEM)

The surface morphology observation was performed on cryogenically fractured samples, on surface etched samples and tensile fractured surfaces using a JSM-7001F scanning electron microscope (JEOL, Tokyo, Japan) operated at 2 kV. Prior to SEM analysis all samples were sputter coated with a thin platinum-palladium (80:20) layer.

2.6. Selective surface etching and image analysis

According to the methodology proposed by Kakroodi *et al.* [2], the etching procedure performed on the cryogenically fractured surfaces was as follows. Samples were etched in a water-methanol solution (1:2 vol./vol.) containing 0.025 mol·L⁻¹ of sodium hydroxide for 7 days at RT, rinsed with distilled water and then dried at 23 °C for 2 days before SEM observations. An open-source software (ImageJ version 1.51 p) was used for image analysis. The weight-average particle diameter $\bar{d}_w$ was determined from a representative surface area of 108 μm^2 according to Equation (1):

$$\bar{d}_w = \frac{\sum n_i d_i^2}{\sum n_i d_i} \quad (1)$$

where n is the number of particles having diameter d .

2.7. Wide-angle X-ray scattering (WAXS)

WAXS measurements were carried out on a Bruker D8 Advance diffractometer (Billerica, MA, USA) with CuK α radiation of wavelength of 1.54 Å. 2D-WAXS patterns were recorded in the range 5–35° (step size = 0.02, scanning speed = 1 s/step) using a PSD LynxEye detector at room temperature.

2.8. Contact angle measurements and surface free energy calculation

The contact angles of distilled water (polar liquid) and diiodomethane (dispersion liquid) were measured by an optical contact angle measuring and contour analysis system (DataPhysics Instruments GmbH, Filderstadt, Germany) using the sessile drop method. The static drops had a volume of 3 μL . At least 8 measurements were done for each sample at a temperature of 22±1 °C. The surface free energy of PLA, PLA_{REx} and PA and their polar and dispersive components were determined according to Equation (2) using the Owens-Wendt method [13, 14]:

$$\gamma_l(1 + \cos(\theta)) = 2\sqrt{\gamma_s^d \gamma_l^d} + 2\sqrt{\gamma_s^p \gamma_l^p} \quad (2)$$

where γ_l is the surface tension of the liquid, θ is the contact angle and γ_s is the surface tension of the solid, also referred to as surface free energy. Superscripts 'd' and 'p' denote the dispersive and polar component of the surface free energy. Water: $\gamma_l^d = 21.8 \text{ mJ/m}^2$, $\gamma_l^p = 51 \text{ mJ/m}^2$; diiodomethane: $\gamma_l^d = 48.6 \text{ mJ/m}^2$, $\gamma_l^p = 2.2 \text{ mJ/m}^2$ [15].

2.9. Tensile testing

The mechanical characterization was performed at both low and high strain rates in order to evaluate the tensile and fracture behaviours, respectively. Type 1BA dumbbell specimens according to ISO 527-2 were rapidly extracted from the compression moulded plates after processing in order to avoid excessive defects during punching. Prior to testing, all samples were stored at RT during one week in order to drive the physical aging process closer to equilibrium. All experiments were performed at RT and a relative humidity content of 50%.

The uniaxial tensile behaviour was assessed according to ISO 527 using a Zwick Roell Z010 testing machine (Zwick Roell, Ulm, Germany) equipped with a 10 kN load cell. A minimum of five specimens were tested at a constant crosshead speed of $10 \text{ mm} \cdot \text{min}^{-1}$ whereas the Young's modulus (E) was determined at $1 \text{ mm} \cdot \text{min}^{-1}$. Young's modulus (E), tensile strength (σ_m), strain at the maximum stress (ϵ_m) and strain at break (ϵ_b) were determined from the engineering stress-strain curves.

2.10. Tensile-impact testing

The fracture behaviour was evaluated through tensile-impact tests using a Resil Impactor Junior pendulum impact tester (CEAST, Italy) following the ISO 8256 method A. The striker had a reduced mass of 3.65 kg, the impact speed was $1.92 \text{ m} \cdot \text{s}^{-1}$ and the nominal impact energy was 6.75 J. A minimum of 10 unnotched specimens were tested in order to report the tensile-impact strength (a_{tU}).

3. Results and discussion

It is well known that the morphology of polymer blends is directly related to the rheological behaviour of their individual components. Therefore, the flow behaviour of the three raw materials was determined in order to predict the composition of the blend where phase inversion occurs. Figure 1 compares the viscosity shear rate dependence for the selected PLA and PA grades to that of PLA_{REx} at 210 °C; i.e. compounding and compression-moulding temperature. The shear viscosity was related to the absolute value of the complex viscosity, determined using dynamic frequency sweeps, assuming the validity of the Cox-Merz rule [16].

PLA exhibits the typical behaviour of linear polymers (i.e. typical pseudoplastic fluid behaviour), while the PA shows pronounced shear-thinning flow

Figure 1. Influence of the reactive processing on the viscosity shear rate dependence of PLA_{REx}.

behaviour. Even though PA exhibits a lower MW than PLA (c.f. Table 2), the PA shear viscosity is considerably higher than that of PLA over the entire range of shear rate investigated. This may be ascribed to the intermolecular interactions between the PA macromolecular chains (i.e. Van der Waals forces between the amide groups), which increase the fluid friction and render PA more viscous than PLA [17]. This behaviour is indicative of a viscosity ratio $\lambda = \eta_{PA}/\eta_{PLA} > 1$. In other words, PLA/PA blends are likely to form a dispersed morphology having PLA as the continuous phase and PA as the discrete phase (i.e. droplets).

Among the available models to predict the phase inversion composition $\phi_{2,PI}$, the so-called Paul and Barlow equation is the most commonly used approach [18–20]. The validity of this basic equation which describes $\phi_{2,PI}$ in terms of volume fractions and viscosities was largely confirmed in several studies for immiscible polymeric blends with λ near unity [21–23]. Nevertheless, large discrepancies between $\phi_{2,PI}$ predictions and morphological observations were reported for blend systems with significant viscosity differences [21, 24–26]. In the present work, the Utracki model [24] was preferred to predict $\phi_{2,PI}$ since $\lambda = \eta_{PA}/\eta_{PLA} > 1$. This model has been already successfully used to predict $\phi_{2,PI}$ for blends with λ different from unity [21, 24–26]. This approach is based on the ‘intrinsic viscosity’ $[\eta]$ and the maximum packing volume fraction ϕ_m given by Equation (3):

$$\lambda = \left[\frac{\phi_m - \phi_{2,PI}}{\phi_m - \phi_{1,PI}} \right] [\eta] \phi_m \quad (3)$$

where $\lambda = \eta_{PA}/\eta_{PLA}$ at the shear rate used for blend preparation, $\phi_{2,PI}$ is the volume fraction at the phase

inversion of the PLA or PLA_{REX} phase, respectively and $\phi_{2,PI} = 1 - \phi_{1,PI}$.

In the range $0.1 \leq \lambda \leq 10$, Equation (3) expanded into the MacLaurin's series and truncated after the second term can be approximated as shown in Equation (4):

$$\phi_{2,PI} = \frac{1 - \frac{\log \lambda}{|\eta|}}{2} \quad (4)$$

Based on published data of the points of phase inversion of several thermoplastics and rubbers, Utracki reported that the optimum value for $|\eta|$ is 1.9 [24]. The shear viscosity at approximately 55 s^{-1} was chosen to calculate λ as it was considered representative of the maximum shear rate at a rotor speed of 50 rpm in the Brabender batch mixer employed. Specifically, the maximum shear rate was estimated using the methodology developed by Bousmina *et al.* [27]. Regarding PLA/PA bio-blends, the estimated value of $\phi_{2,PI}$ indicates that the composition of phase inversion is about 38 vol% of PLA (c.f. Table 2). Thus, the theoretical point of phase inversion is reached at a rather low PLA weight fraction $W_{2,PI}$ of 42 wt%.

The fundamental challenge is to shift $\phi_{2,PI}$ towards higher PLA contents in order to manufacture PLA/PA bio-blends with a predominant PLA content. Accordingly, the PLA flow behaviour was modified through reactive extrusion using a multifunctional epoxide. As can be seen in Figure 1, PLA_{REX} exhibits a significantly higher shear viscosity over the whole experimental window as compared to PLA. The former equally presents pronounced shear-thinning flow behaviour similar to that of PA. This difference is ascribed to the alteration of the molecular mobility due to the chemical reactions which may take place between the PLA functional end groups and the

epoxy ring of the chain extender. Since SAMfE is a multifunctional reactive agent, several PLA chains may be chemically bound to one SAMfE molecule through chain extension or branching reactions, as already reported elsewhere [28]. The complex topological modifications generated coupled with an increasing number of interactions and entanglements per chains (i.e. higher M_w , c.f. Table 2) led to a decreasing rate of molecular relaxation, thus enhancing the PLA_{REX} flow properties.

PLA_{REX} exhibited similar η values at 55 s^{-1} as PA, as shown in Figure 1. Therefore, λ was significantly reduced for PLA_{REX}/PA bio-blends; thus shifting the theoretical $\phi_{2,PI}$ to a higher PLA_{REX} content of 56 wt% (c.f. Table 2). Since this current study is focused on bio-blends with a predominant PLA content, five PLA_{REX}/PA blends covering the 10–50 wt% PA composition range were further investigated (c.f. Table 1). PLA/PA bio-blends were equally processed for the sake of comparison.

Since the final blend properties are highly dependent on the induced morphology, SEM observations were carried out on the cryogenically fractured surface of PLA and PLA_{REX}-based bio-blends (Figure 2). Regarding PLA-based bio-blends, SEM micrographs revealed the expected two-phase structure independently of the formulation considered. The sea-island morphology in which droplets of the PA phase were embedded in the continuous PLA matrix confirms the basic immiscible nature of the PLA/PA10.10 bio-blends. Increasing the PA content apparently seems to induce a growth of the average drop size. As noted on the cryofractured surface, each formulation released the triaxial stress state induced during fracture by voiding and second phase particle debonding. This behaviour indicates a poor interfacial adhesion between both components.

Table 2. Technical specifications for the three raw materials used in this study.

Material code	T_{mp}/T_{me}^a [°C]	M_n/M_w^b [kDa]	MFI at 210 °C, 2.16 kg [g/10 min]	η at $\dot{\gamma} = 55 \text{ s}^{-1}$, 210 °C [Pa·s]	λ^d at $\dot{\gamma} = 55 \text{ s}^{-1}$	$\phi_{2,PI}$ [vol%]	$W_{2,PI}^e$ [wt%]
PLA	167/173	90/181	6.4±0.3	504	2.74	38	42
PLA _{REX}	165/171	121/290	1.1±0.1	1567	0.88	52	56
PA	200/206	11/33	— ^c	1383	—	—	—

^aPeak melting temperature (T_{mp}) and end melting signal temperature (T_{me}) determined using DSC experiments from the second heating cycle at $10^\circ\text{C}\cdot\text{min}^{-1}$.

^bRelative values determined using SEC-DRI experiments.

^cNot determined for this material.

^d $\lambda = \eta_{PA}/\eta_{major\ phase}$, being PLA or PLA_{REX} the major phase for PLA and PLA_{REX}-based bio-blends, respectively.

^eThe densities of PLA/PLA_{REX} and PA were 1.24 and 1.05 g/cm³, respectively.

Figure 2. SEM micrographs ($\times 10\,000$) of the cryofractured surfaces of PLA and PLA_{REX} based bio-blends, respectively. Continuous domains of PA are highlighted within the red dashed lines. Scale bars = 2 μm .

Figure 3. SEM micrographs of the cryofractured surfaces of PLA and PLA_{REX} based bio-blends after surface etching. Regarding PA composition in the range 10–30 wt%, scale bars = 2 μm (×10 000). For 60/40 and 50/50 formulations, scale bars = 20 μm (×1500).

In contrast, the cryofractured surface morphology of PLA_{REX}-based bio-blends did not display any clear evidence of phase-separated domains. Moreover, the rare and smaller PA drops which were found on the fracture surface of the PLA_{REX}90, PLA_{REX}80 and PLA_{REX}70 formulations seemed to be covered with matrix. This observation suggests a better interfacial adhesion between both polymers. When the PA content increased up to 40 wt% continuous domains of PA appeared (indicated within the red dashed lines in Figure 2), suggesting that this formulation was at the onset of co-continuity. Nevertheless, the analysis of PLA_{REX}/PA SEM micrographs suffered from the intrinsic two-dimensional feature of the image coupled with the poor separation between both polymers. Thus, possibility of misinterpreting the blend morphology is largely expected. To substantiate the previous observations, surface etching of the PLA_{REX} matrix was performed to provide an insight into the PA morphology in PLA_{REX}/PA bio-blends. For comparison purposes, PLA/PA bio-blends were equally surface etched using the same conditions.

Figure 3 shows the dispersion of the remaining PA phase after the PLA and PLA_{REX} selective surface etching, respectively. Regarding PLA-based bio-blends in the composition range of 90–70 wt%, it can be seen that the PLA matrix remained visible in the corresponding micrographs of the etched surfaces. This observation suggests that the near-spherical PA droplets were non-uniformly suspended in the PLA matrix and were not self-supported during the etching process. As can be seen in Table 4, increasing the PA content from 10 to 30 wt% significantly increased the weight-average particle diameter from initially 0,7 to 2,6 μm . The etched surface of the PLA60 formulation shows the coexistence of spherical PA droplets with some coarse elongated structures. Finally, the dispersed PA phase featured solely coarse elongated domains when the PLA content was decreased to 50 wt%.

Significant morphological changes occurred with the modification of the PLA flow behaviour. In the PLA_{REX} composition range 90–80 wt%, the PA dispersed droplets were much finer and more homogeneously dispersed than PLA-based bio-blends, as shown in Figure 4. Increasing the PA content also increased the weight-average particle diameter but to a much lesser extend as compared to their PLA counterpart. $\bar{d}_w$ increased from initially 0.19 to 0.24 μm . To the best of our knowledge similar size of the PA

Figure 4. Quantitative analyses of the PA weight-average particle diameter, $\bar{d}_w$, in PLA and PLA_{REX} composition a) 90/10, b) 80/20. Inserts show a detailed view of the PA particle diameter distribution for PLA_{REX}-based bio-blends.

disperse phase in PLA/PA systems has only been reported by Kakroodi *et al.* [2] for thin PA6 microfibrils in a two-step hot stretching process. In this study, the observed morphological improvement must be primarily attributed to the higher shear viscosity of the PLA_{REX} matrix during compounding. That is, the enhanced $\eta_{\text{PLA}_{\text{REX}}}$ possibly increased the local shear field applied to the initial coarse PA domains; thus enabling further PA droplet breakup and minimizing coalescence during mixing. Similar observations have been already reported by Lee *et al.* [9] regarding the evolution of blend morphology in different blend systems.

When the PA content was 30 wt% both droplet and elongated PA domains coexisted. The morphology transition to co-continuous was completed when the PA content was further increased to 40 wt%. Irregularly shaped PA domains interpenetrated the PLA_{REX} major phase in the PLA_{REX}60 formulation. These observations are in agreement with the initial rheological predictions. Finally, elongated PLA_{REX}

Figure 5. WAXS profiles for all manufactured materials.

domains in PA were revealed for the PLA_{REX}50 sample.

It is well known that mechanical performances of polymer systems are highly dependent on the crystallinity induced during manufacturing. On this basis, WAXS experiments were performed on all the compression moulded samples. WAXS patterns recorded for PLA and PLA_{REX} based bio-blends are compared in Figure 5. PLA and PLA_{REX} intensity profiles do not display any crystalline reflections, which indicate that both processed neat samples were amorphous under the processing conditions used in this study. These observations are in agreement with the slow kinetics of crystallization exhibited by both materials, as already reported elsewhere [29, 30]. Nevertheless, a small diffraction peak at $2\theta = 16.4^\circ$ corresponding to PLA α form crystallinity [2] can be seen for the 90/10 and the 80/20 blends, being more prominent in the case of PLA-based blends. This indicates that the presence of small amounts (10–20 wt%) of PA10.10 acted as a heterogeneous nucleating agent and formed a small PLA crystal fraction in these blends. Indeed, Kakroodi *et al.* [2] showed that micron- and sub-micron-sized PA domains dispersed in PLA matrix increased the PLA crystallization rate. Nevertheless, no such effect was seen for higher PA contents. In contrast, the monoclinic α crystal phase of neat PA samples was present through the peaks at about $2\theta = 20.5$ and 23.5° [31]. Analogously, PLA

and PLA_{REX} based bio-blends display these diffraction peaks corresponding to the PA crystal form.

The mechanical properties of polymer blends further depend on the interfacial adhesion between the polymer phases. The contact angle of polymers mainly depends on their chemical structure and surface roughness and is characteristic for their hydrophilic properties and thus their wettability of other polymers [13, 14].

The results of the surface contact angles and the surface free energy calculations of PA, PLA and PLA_{REX} are shown in Figure 6 and Table 3. Comparing PLA and PLA_{REX}, the water contact angle dropped from 75° to 63° , suggesting a more hydrophilic nature of PLA_{REX}. The surface energy of PLA calculated according to the Owens-Wendt method was 42.6 mJ/m^2 which agreed well with published values from other researchers [14, 32]. The reactive extrusion of PLA and multifunctional epoxide reactive agent (i.e. PLA_{REX}) increased the surface energy to 51.5 mJ/m^2 . This enhancement was due to the large increase in the dispersive component while the increase in the polar component was not significant. The increased surface energy of PLA_{REX} resulted in less interfacial

Figure 6. Water and diiodomethane contact angles of PA, PLA and PLA_{REX}.

Table 3. Average contact angles and surface free energies of PA, PLA and PLA_{REX}.

Sample	Contact angle θ water [°]	Contact angle θ diiodomethane [°]	Surface energy [mJ/m ²]	Dispersive component [mJ/m ²]	Polar component [mJ/m ²]
PA	86 ± 2	27 ± 2	46.4	45.4	1.1
PLA	75 ± 2	48 ± 3	42.6	35.4	7.2
PLA _{REX}	63 ± 3	30 ± 3	51.5	44.2	7.3

tension during blending with PA and consequently led to a size reduction of the dispersed phase and a better interfacial adhesion as compared to PLA blends. Representative tensile engineering stress-strain curves for both types of bio-blends are shown in Figure 7. The tensile properties are compiled in Table 4 and Figure 8. Both PLA and PLA_{REx} exhibited similar properties, namely a high stiffness and strength coupled with brittleness (i.e. low strain at break). For both PLA

and PLA_{REx} blends the stiffness and strength decreased gradually from around 2.3 to 1.3 GPa and from 63 to 48 MPa, respectively, when the PA content increased. The strain at break of the PLA_{REx}-based bio-blends increased also significantly with increasing PA content. However, the 90/10 blends showed a higher modulus as compared to their corresponding PLA matrix. Recall that according to WAXS results this blend exhibited a small PLA crystal

Figure 7. Typical uniaxial tensile engineering stress-strain curves for PLA (a) and PLA_{REx} (b) based bio-blends.

Table 4. Uniaxial tensile properties, tensile impact strength a_{tU} and PA weight-average particle diameter $\bar{d}_w$.

Sample	E [GPa]	σ_m [MPa]	ε_b [%]	a_{tU} [kJ·m ⁻²]	$\bar{d}_w$ [μm]*
PLA	2.3±0.1	63±1	2.5±0.3	102±20	n/a
PLA _{REx}	2.6±0.2	64±1	3.2±0.1	106±11	n/a
PA	1.5±0.1	46±1	155±27.0	459±65	n/a
PLA-based bio-blends					
PLA90	2.9±0.2	61±2	2.2±0.1	68±5	0.702
PLA80	1.8±0.1	58±2	3.6±0.8	111±16	1.752
PLA70	1.8±0.1	57±1	28±5.0	145±12	2.551
PLA60	1.4±0.2	50±1	142±39.0	221±39	n/a
PLA50	1.3±0.1	48±1	117±60.0	221±55	n/a
PLA_{REx}-based bio-blends					
PLA _{REx} 90	2.7±0.1	66±1	18±12.0	98±23	0.186
PLA _{REx} 80	2.2±0.1	60±1	166±9.0	126±6	0.241
PLA _{REx} 70	2.0±0.2	58±1	144±15.0	174±27	n/a
PLA _{REx} 60	1.4±0.2	51±1	162±32.0	280±43	n/a
PLA _{REx} 50	1.3±0.1	49±1	173±26.0	333±39	n/a

*The weight-average particle diameters were only calculated for formulations exhibiting near-spherical PA droplets.

Figure 8. Effect of the PA content on the strain at break (column bar) and maximum stress (scatter) for both types of bio-blends.

fraction which was absent in blends with higher PA content. This PLA crystal fraction might account for the relatively higher stiffness of this blend.

Regarding the failure strain, a semi-ductile behaviour was observed for the PLA_{REX}90 formulation and

strain at break values well above 100% were measured for higher PA contents. On the other hand, the PLA-based bio-blends did not show this behaviour. The addition of 10 or 20 wt% of PA did not affect the PLA brittleness. A semi-ductile behaviour was observed for the PLA70 blend and strain at break values were above 100% for PA contents of 40 wt% or higher. The relatively large scatter in the failure strain data of PLA-based blends with high PA content is due to the unstable necking of the tensile specimens. This was ascribed to the relatively coarser microstructure featuring large PA particles which led to premature failure. To sum up, an apparent brittle-to-ductile transition was observed when the PA content in PLA-based bio-blends was 30 wt%. In PLA_{REX}-based blends this transition was achieved with only 10 wt% of PA. In Figure 9, the SEM morphologies of the fracture surfaces of tensile specimens reflect well this brittle-to ductile transition. For instance, the morphology of the PLA80 bio-blend exhibits a quite

Figure 9. SEM micrographs ($\times 5000$) of the tensile fractured surfaces of PLA- and PLA_{REX}-based bio-blends. Scale bars = 4 μm .

smooth fracture surface together with the tearing and decohesion of PA particles. This suggests a brittle fracture and indeed the observed strain at break was only about 4%. In contrast, the fractured surface of the PLA_{REX}80 bio-blend does not display any particle decohesion mechanism. Under tensile loading the smaller and homogeneously dispersed PA droplets allow a significant release of the triaxial stress state in the matrix, thus allowing the specimen to undergo shear yielding.

The SEM images of the PLA70 and PLA50 bio-blend featured a typical fibrillated structure originated from the ductile tearing of the larger PA particles. It is not surprising that a certain extend of fibril debonding can equally be observed due to the poor interfacial adhesion between both polymers. These observations confirm the observed semi-ductile and/or ductile behaviour of these blends. In contrast, stretched fibrils appeared to be more uniform for PLA_{REX}70 based bio-blend due to the finer dispersion of the initial PA droplets combined with the presence of microfibrils, thus greatly enhancing the toughness of this formulation. Finally, PLA_{REX}50 bio-blends exhibited the typical fracture surface features of phase inverted blends.

The PA weight-average particle diameters of the different PLA and PLA_{REX}-based bio-blends featuring only near-spherical PA droplets were determined from the SEM morphologies and are compiled in Table 3. It is apparent that PLA-based blends exhibited relatively large PA particle diameters >1 µm while the particle diameters in PLA_{REX}-based blends were around ten times smaller. The relatively finer microstructure of PLA_{REX} together with its enhanced interfacial adhesion resulted in a ductile behaviour with failure strains well above 100%.

The toughening effect of the dispersed PA on the PLA and PLA_{REX} matrices was also observed in tensile-impact tests (c.f. Table 4). Figure 10 depicts the tensile-impact strength a_{IU} as a function of PA content for the PLA- and PLA_{REX}-based bio-blends. Contrary to what was observed in quasi-static uniaxial tensile tests, the tensile-impact strength increased only marginally and no clear brittle-to-ductile transition was found. The tensile-impact strength of both matrices was not markedly affected up to a PA content of 20 wt% and then gradually increased for higher PA contents due to the ductile behaviour of the increasingly PA secondary phase. This improvement

Figure 10. Tensile-impact strength for PLA and PLA_{REX}-based bio-blends.

was always more pronounced for the PLA_{REX}-based bio-blends due to the morphological improvements as observed in Figure 3.

4. Conclusions

This work shows that PLA/PA bio-blends have the potential to overcome the inherent brittleness of PLA. However, 30 wt% of PA was needed to achieve a brittle-to-ductile transition and a co-continuous morphology was found at 58 wt% of PA due to the immiscible nature of the blend. Unfortunately, increasing the PA fraction significantly reduced the PLA stiffness and strength and also increased the size of the dispersed PA phase.

On the other hand, the initial improvement of the PLA rheological behaviour through reactive extrusion yielded a finer and more homogeneous microstructure and apparently a better interfacial adhesion since the PA dispersed phase was covered with matrix. Consequently, the mechanical properties of the PLA_{REX}/PA bio-blends were enhanced at much lower PA contents. Under uniaxial tensile conditions, the brittle-to-ductile transition could be achieved with only 10 wt% and co-continuity was observed already at 44 wt% of PA. These findings may help to establish PLA_{REX}/PA bio-blends, such as the 80/20 formulation, with high PLA fractions and good toughness without significantly sacrificing stiffness and strength.

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